

Deep CNN for Segmentation of Myocardial ASL Short-Axis Data: Accuracy, Uncertainty, and Adaptability

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Capital Hilton, Washington, D.C., USA

ISMRM Workshop on
Machine Learning
Part II

25-28 October 2018

Chair: Greg Zaharchuk, M.D., Ph.D., Stanford University, Stanford, CA, USA
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Declaration of Financial Interests or Relationships

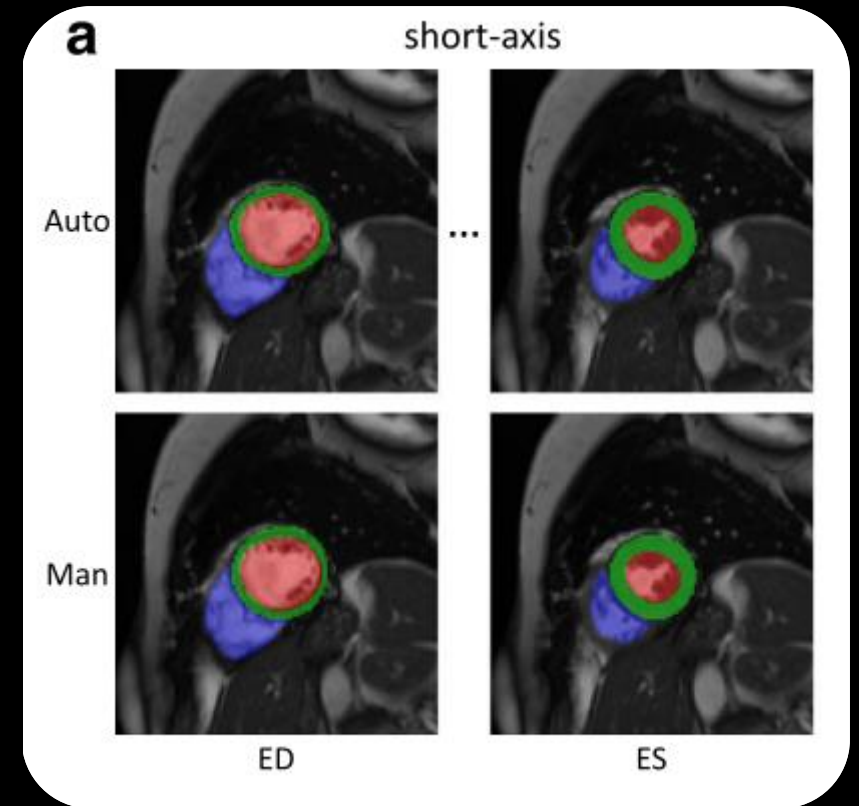
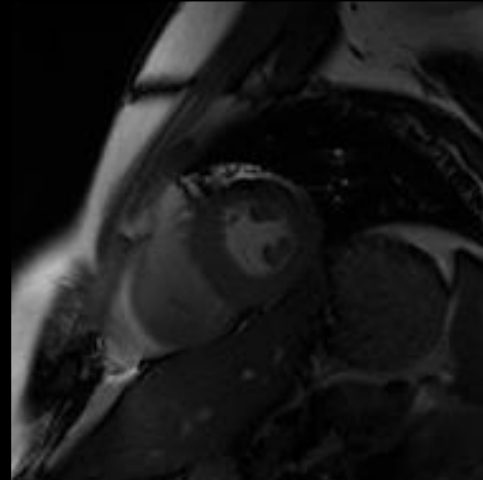
Speaker Name: Hung Do

Company Name: Canon Medical Systems USA, Inc. (formerly Toshiba Medical)

Type of Relationship: Employee

Intro(1): CNN for segmentation

- Comparable to human experts in analyzing cardiac CINE data¹
 - Dice Coef. of 0.94 for LV blood pool
 - Dice Coef. of 0.88 for LV myocardium
 - Dice Coef. of 0.90 for RV blood pool

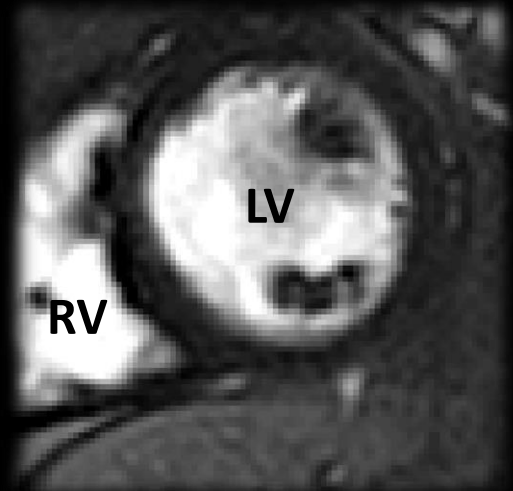


Goals

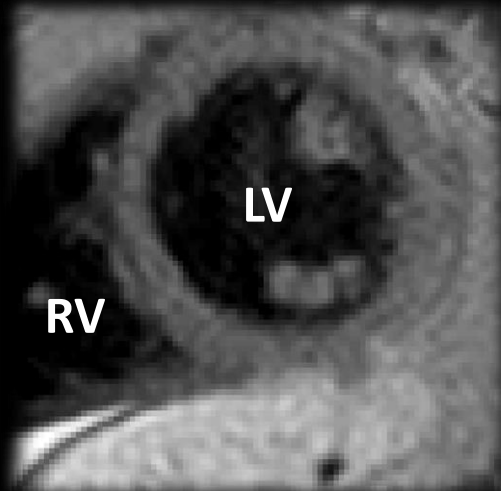
1. To apply CNN for **segmentation** of myocardial Arterial Spin Labeled (ASL) data
2. To measure model **uncertainty** using **Monte Carlo dropout**
3. To **adapt** the CNN model to the desired trade-off between false positive (FP) and false negative (FN) using **Tversky loss** function

Intro(2): Myocardial Arterial Spin Labeling (ASL)

Control Image

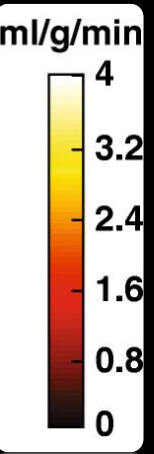
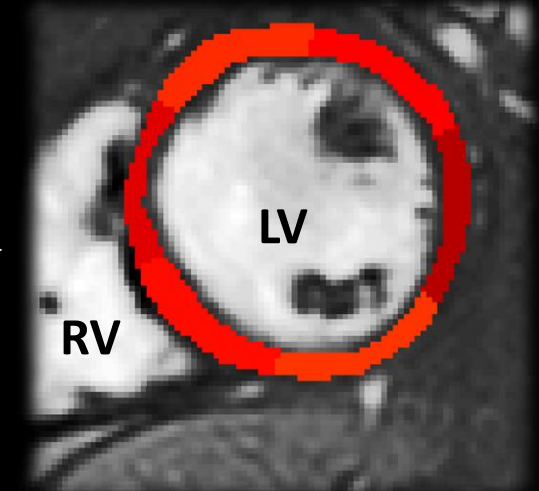


Labeled Image

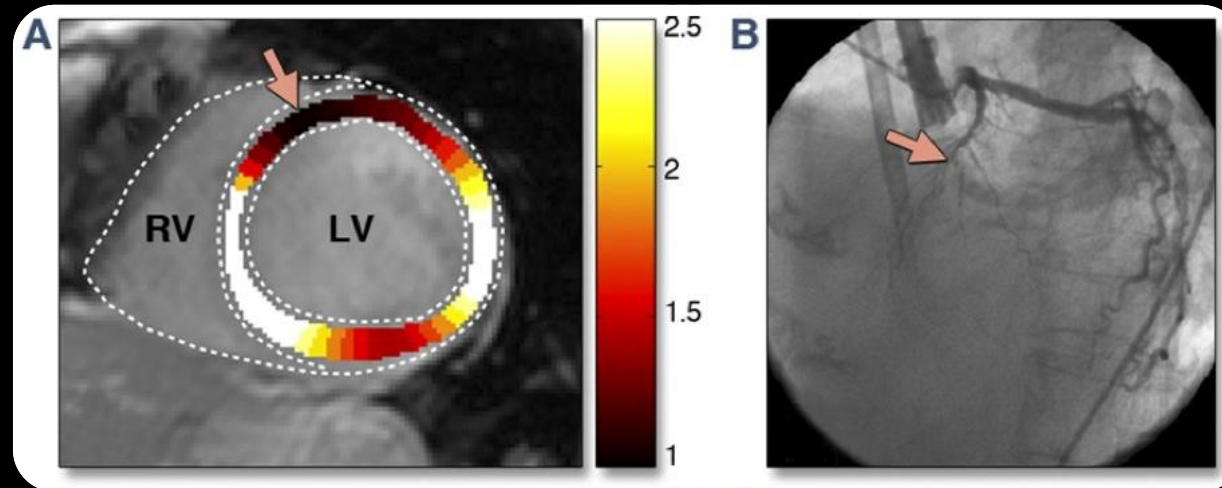


3-5 min
man. seg. of
6 averages

Myocardial Blood Flow (MBF)
(perfusion)



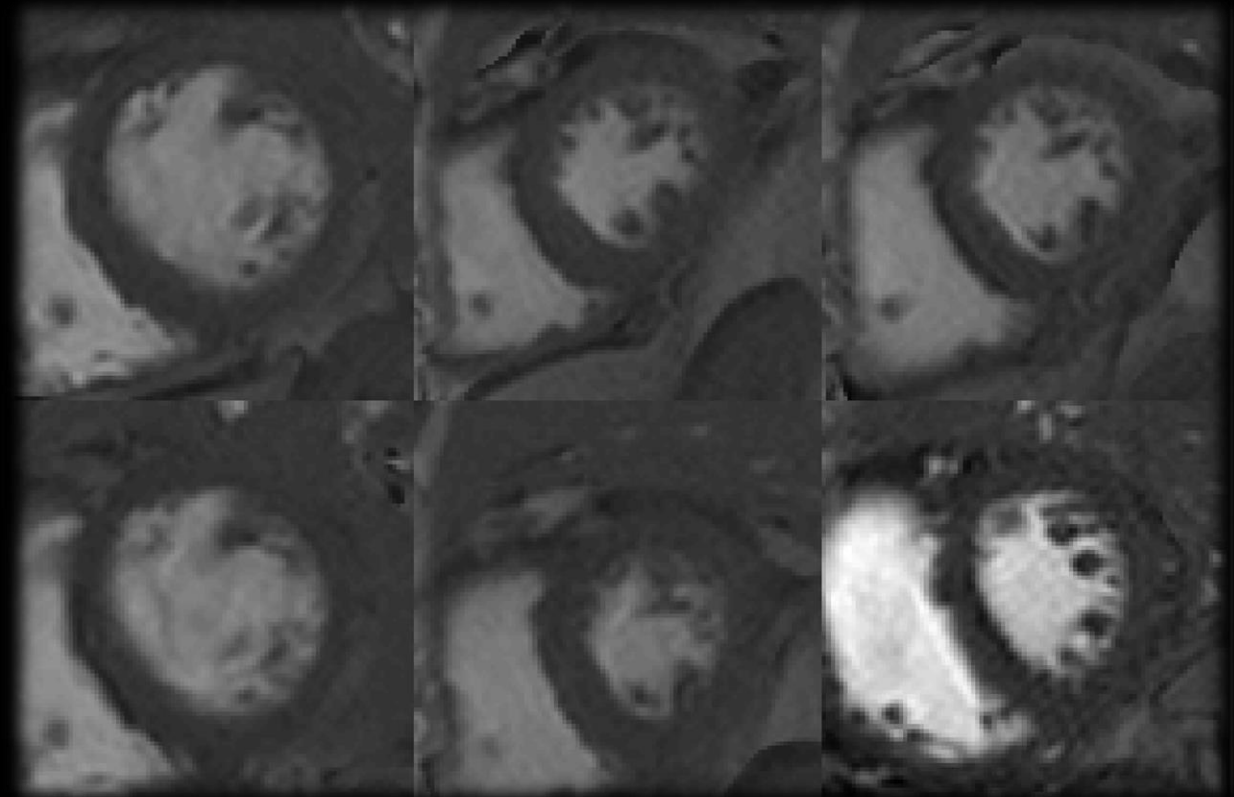
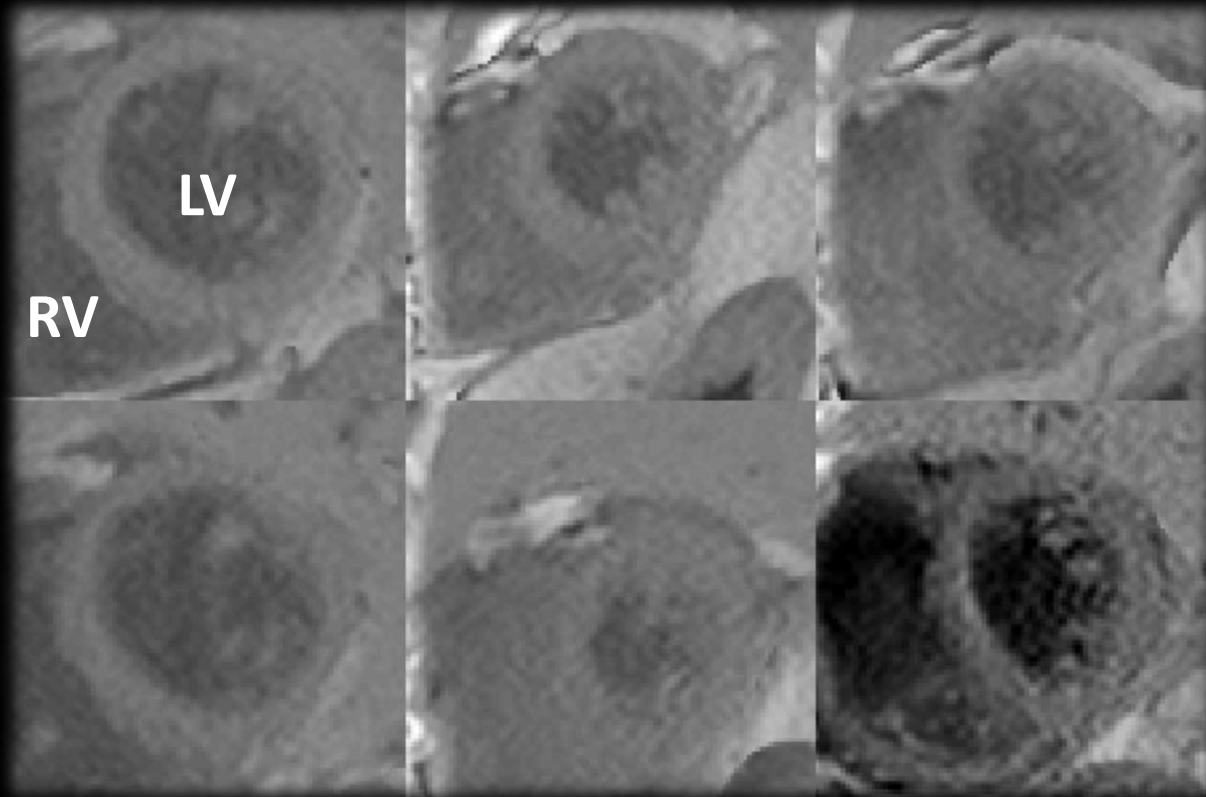
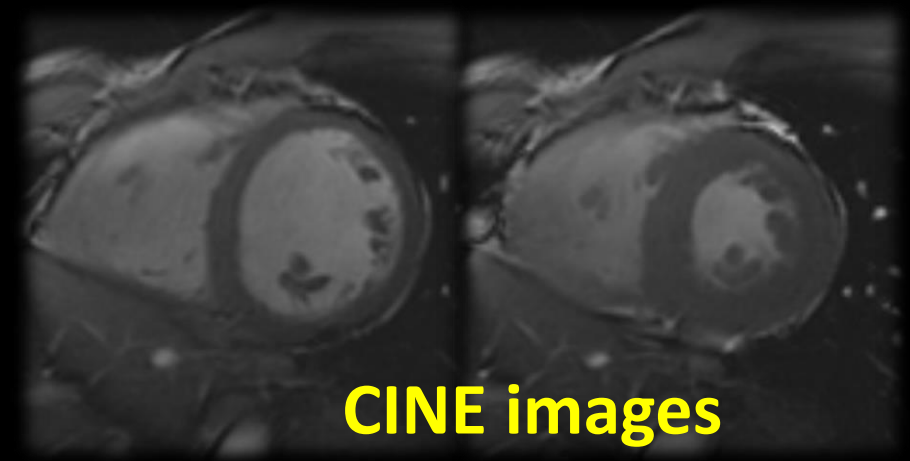
Coronary artery
disease (CAD)



1. Kober, Frank et al. "Myocardial arterial spin labeling." Journal of Cardiovascular Magnetic Resonance 2016; 18:22.
2. Zun, Zungho et al., " ASL-CMR Detects Clinically Relevant Increases in Myocardial Blood Flow With Vasodilation." JACC 2011; 4(12):1253-1261.

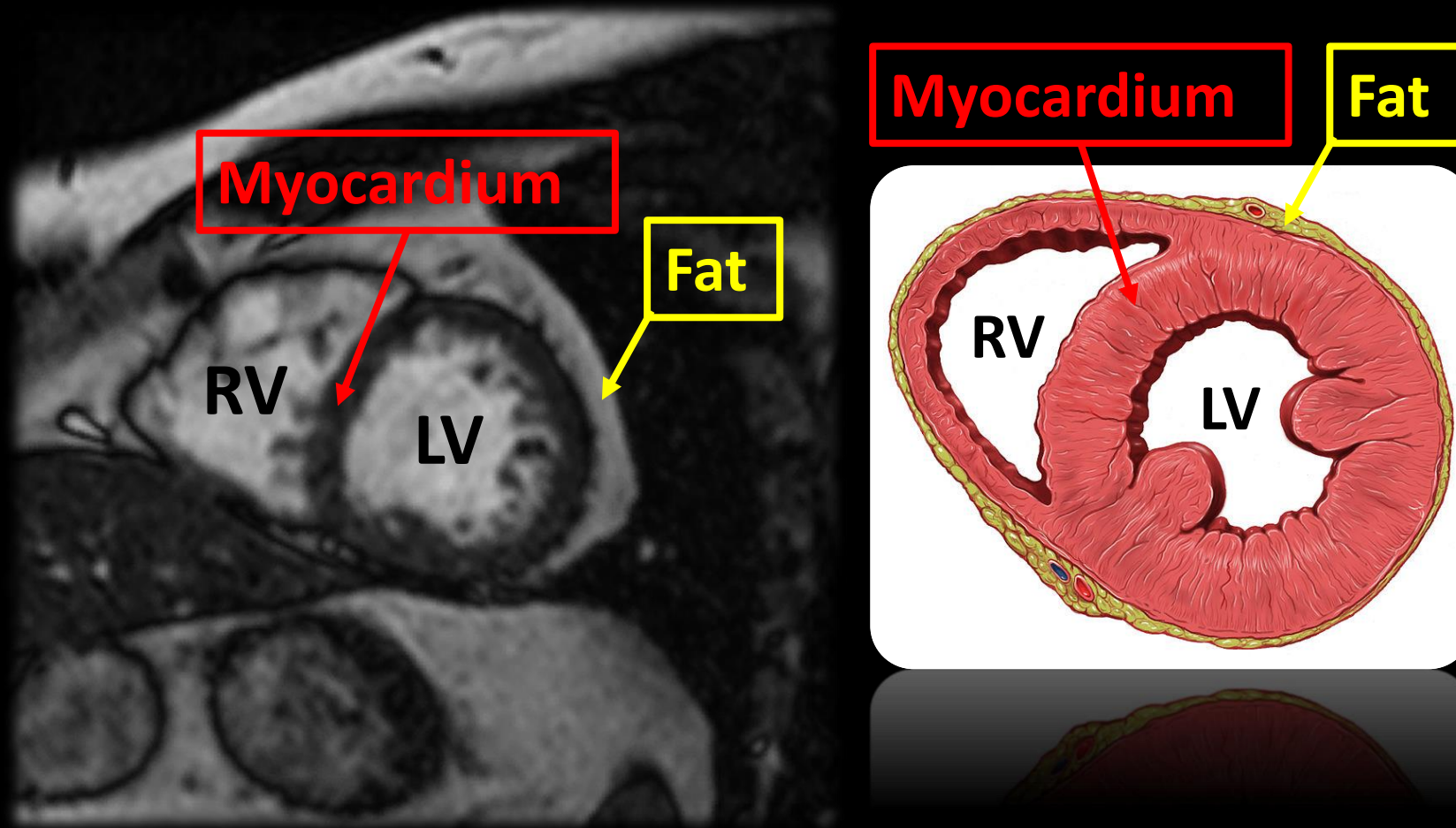
Intro(3): Characteristics of ASL data

- Low resolution
- Low SNR and CNR
- Varying SNR and CNR



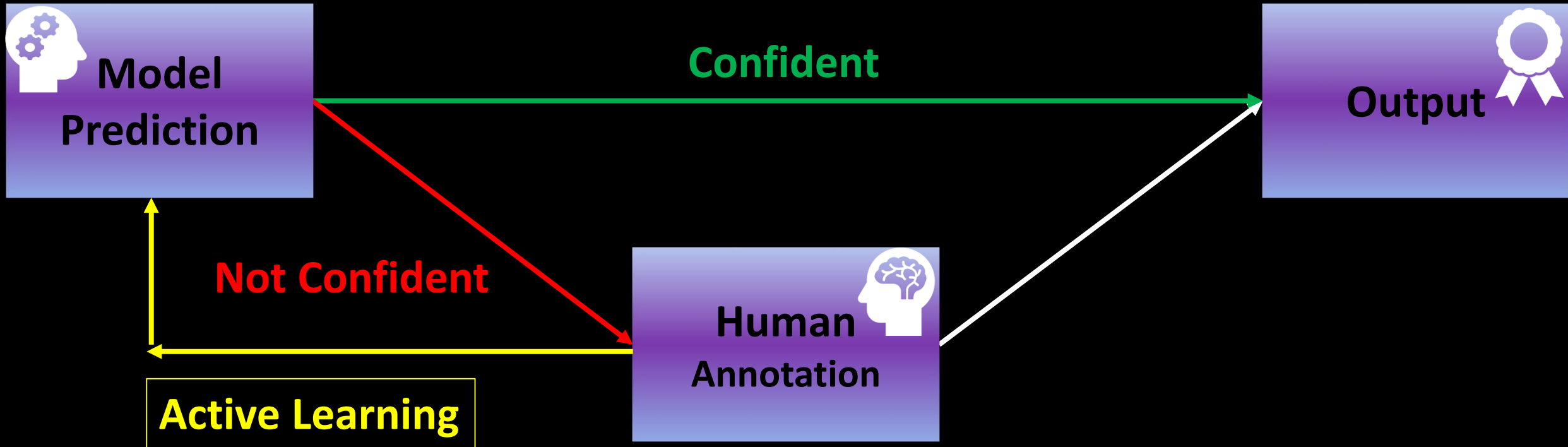
Intro(4): Partial volume effects

- Ventricular blood and epicardial fat have **different physical properties** and **spin history** compared to myocardium.



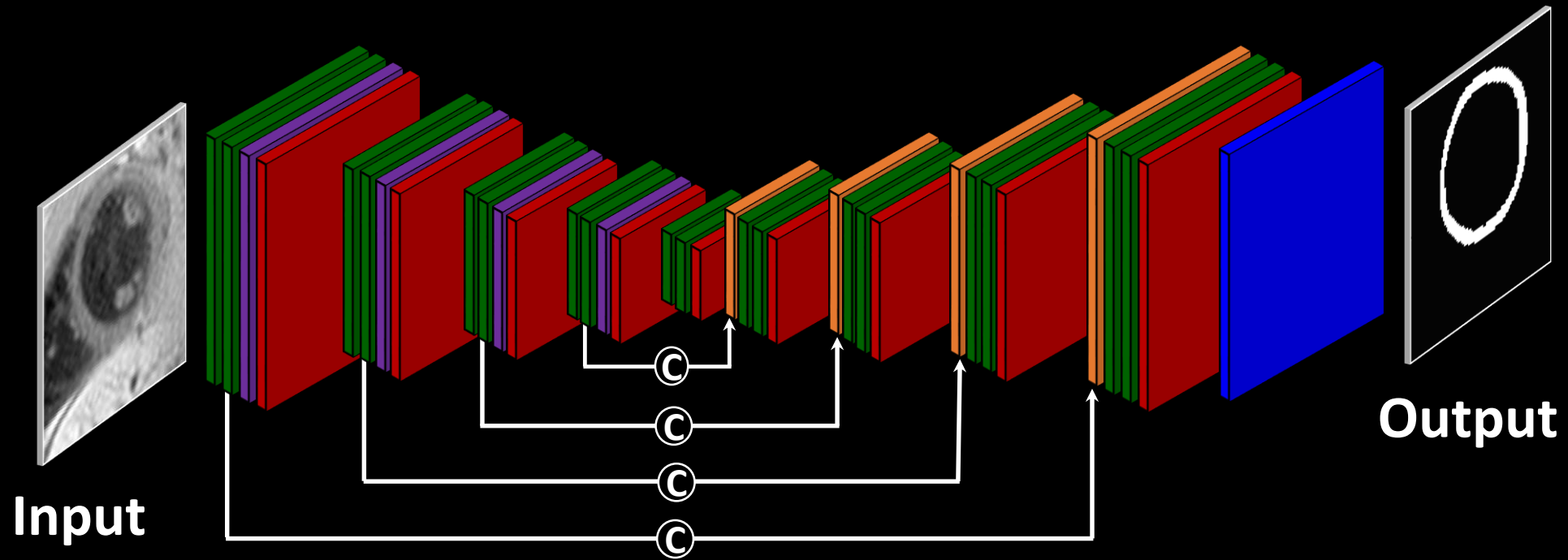
Intro(5): Why model uncertainty?

- Quality control during **production/deployment**
- Model improvement via **active learning**



Methods(1): Network Architecture¹

loss = **Binary Cross-Entropy** or **(1 – Soft-Dice)** or **(1 – Tversky Index)**



 **5x5 Conv+ReLU+BN**  **Max Pooling**  **Monte Carlo Dropout**  **Upsampling**  **1x1 Conv+Sigmoid**

 **Channel Concatenation**

Methods(2): Dataset and training parameters

- Training and validation data¹:
 - From **22 subjects**: 478 images – 438/40 images for training/validation
- Test data¹:
 - From **6 “un-seen” heart transplant patients**: 144 images (rest and during Adenosine stress)
- Training parameters:
 - 150 epochs
 - Learning rate: 1e-4
 - Dropout rate: 0.5
 - Batch size = 12
 - Adam optimizer

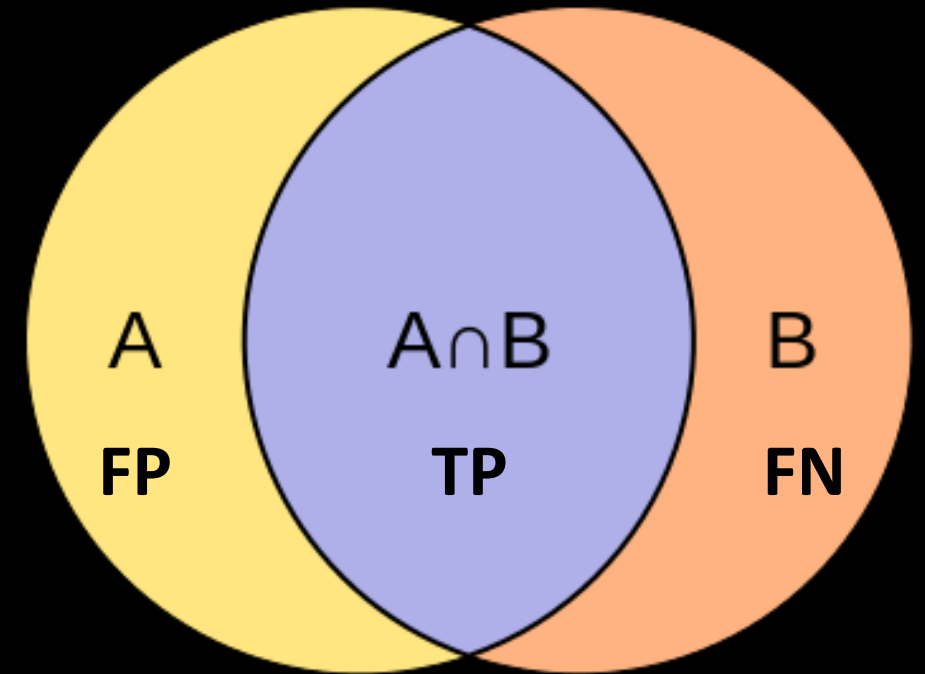
Methods(4): Adaptability using Tversky loss

$$Dice = \frac{2 \cdot |A \cap B|}{|A| + |B|}$$

A: Predicted Mask
B: Reference Mask

$$Dice = \frac{2 \cdot TP}{2 \cdot TP + FP + FN} = \frac{TP}{TP + 0.5 \cdot FP + 0.5 \cdot FN}$$

$$Tversky\ Index = \frac{TP}{TP + (1 - \beta) \cdot FP + \beta \cdot FN}$$



Tversky loss = 1 - Tversky Index¹

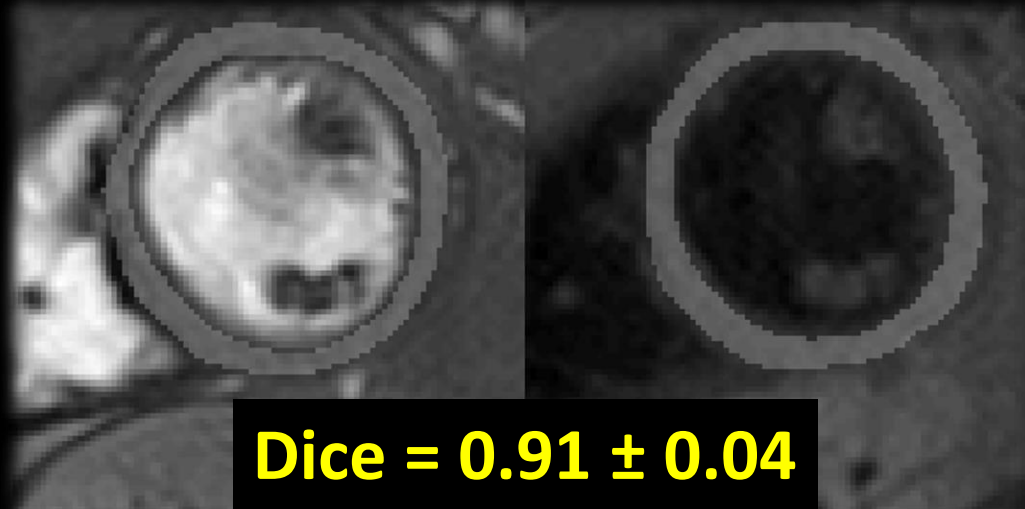
Results(1): Accuracy – Dice Coefficient

Control Image

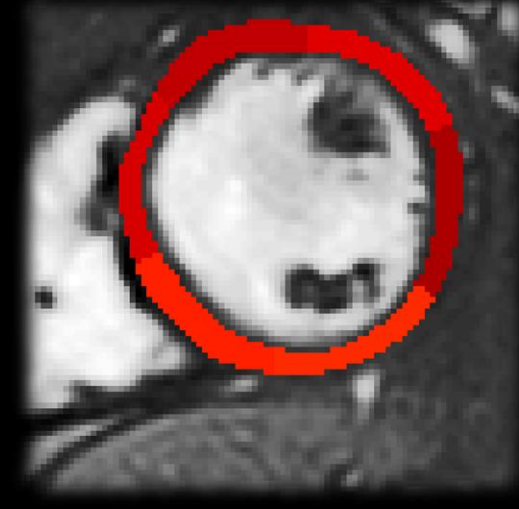
Label Image

Myocardial Blood Flow (MBF)
(perfusion)

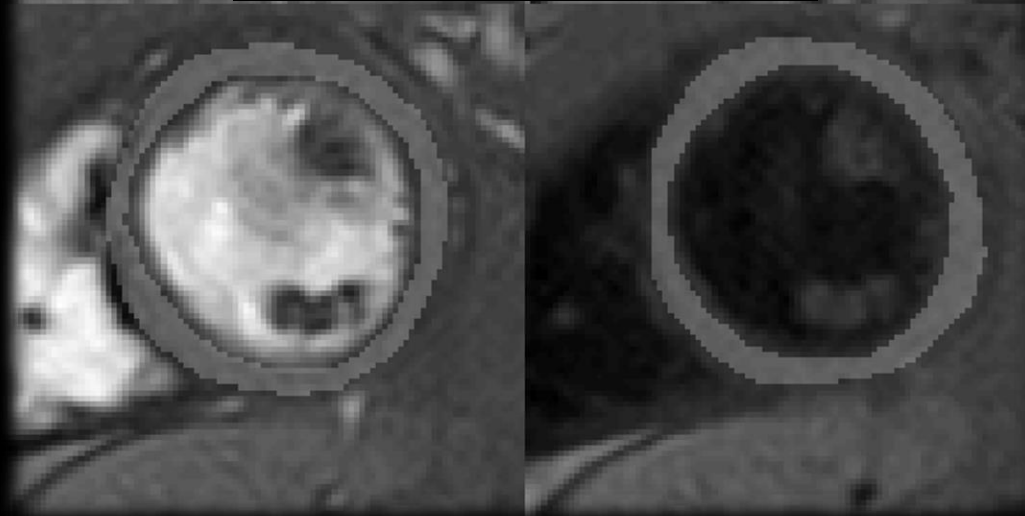
Auto



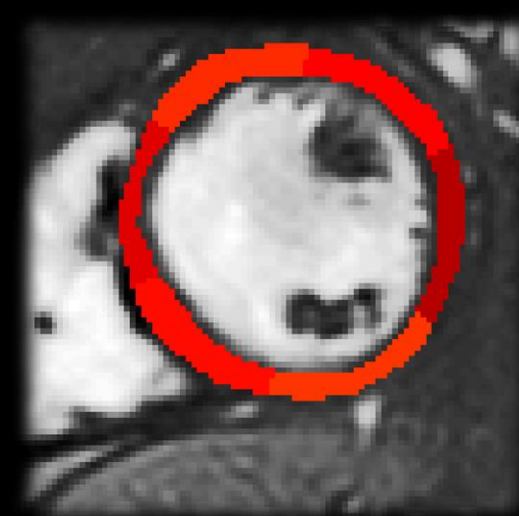
Auto



Man

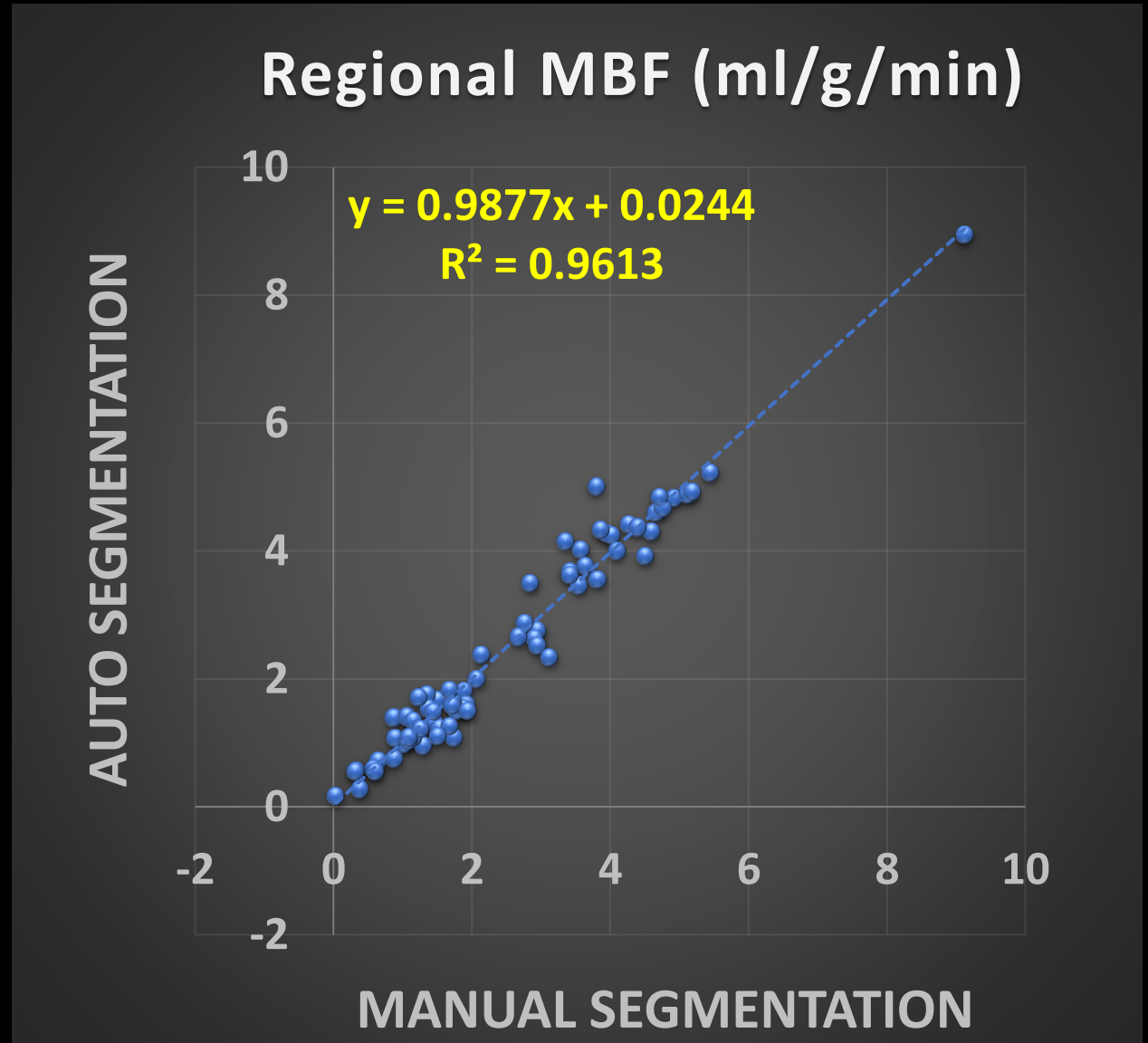


Man



Results(1): Accuracy – Myocardial Blood Flow (MBF)

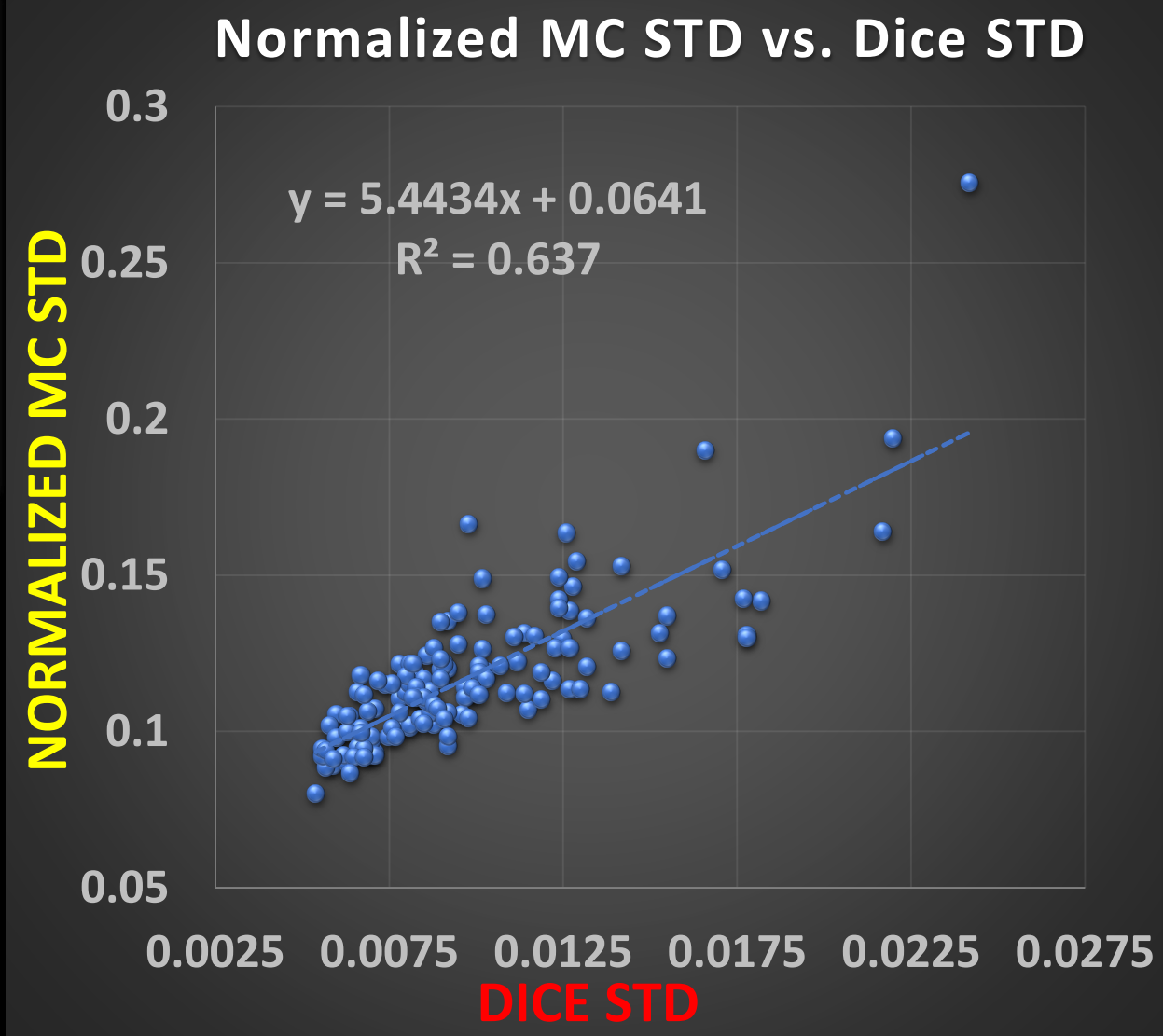
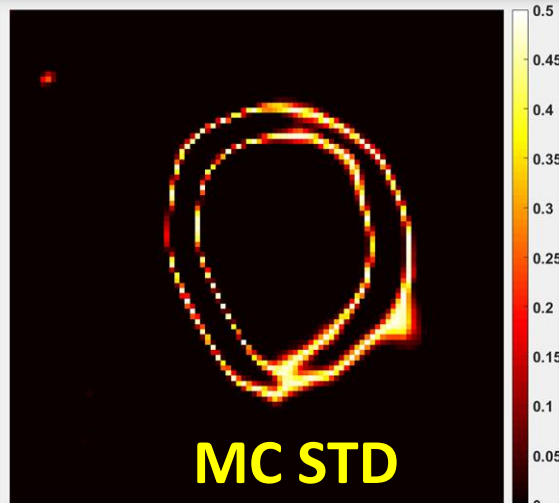
MBF measured using automatic segmentation is **highly correlated** to that measured using manual segmentation



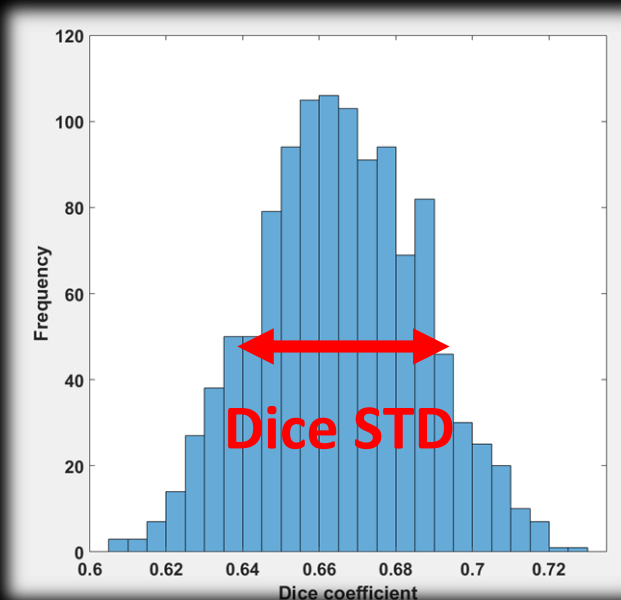
Results(2): Uncertainty

Without manual segmentation

1115 MC trials

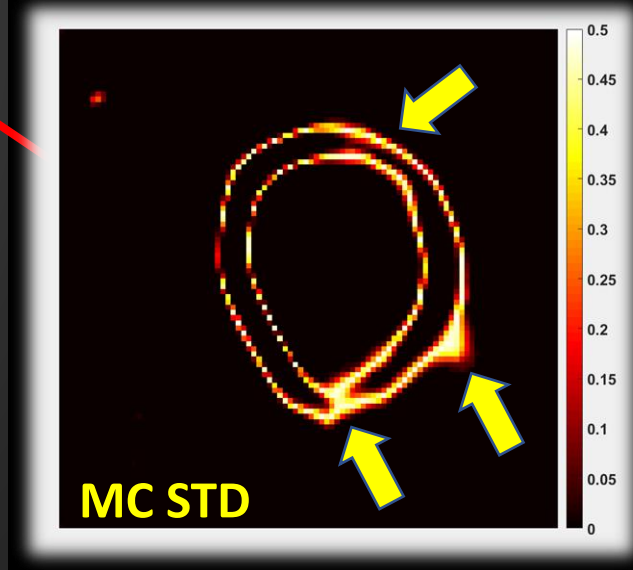
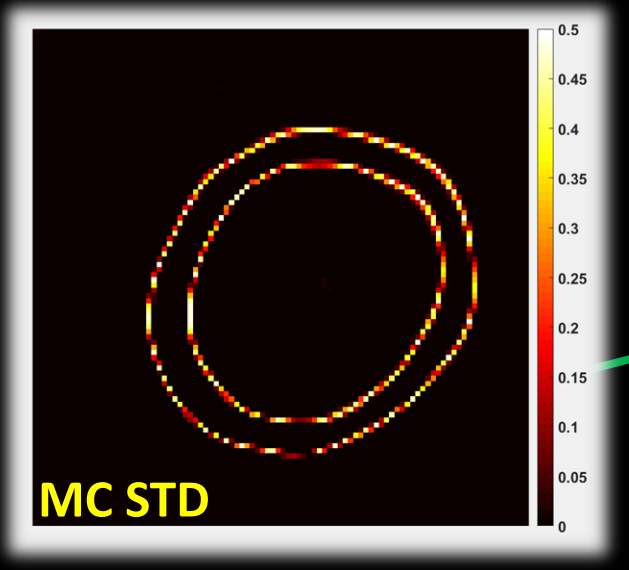
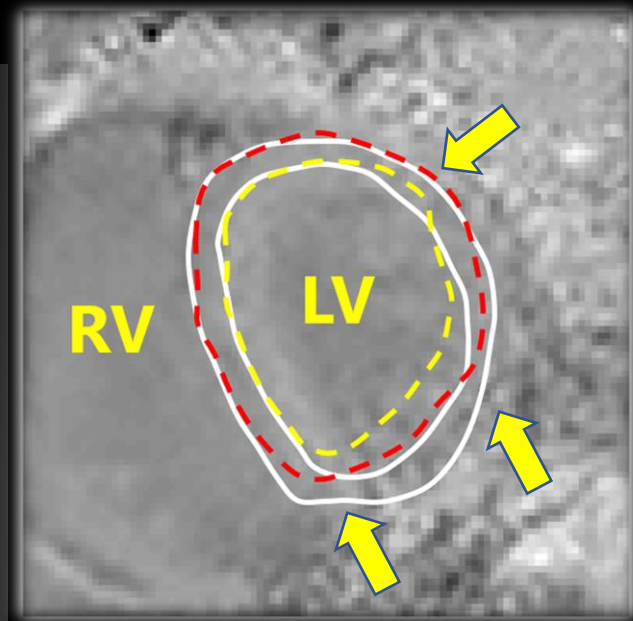
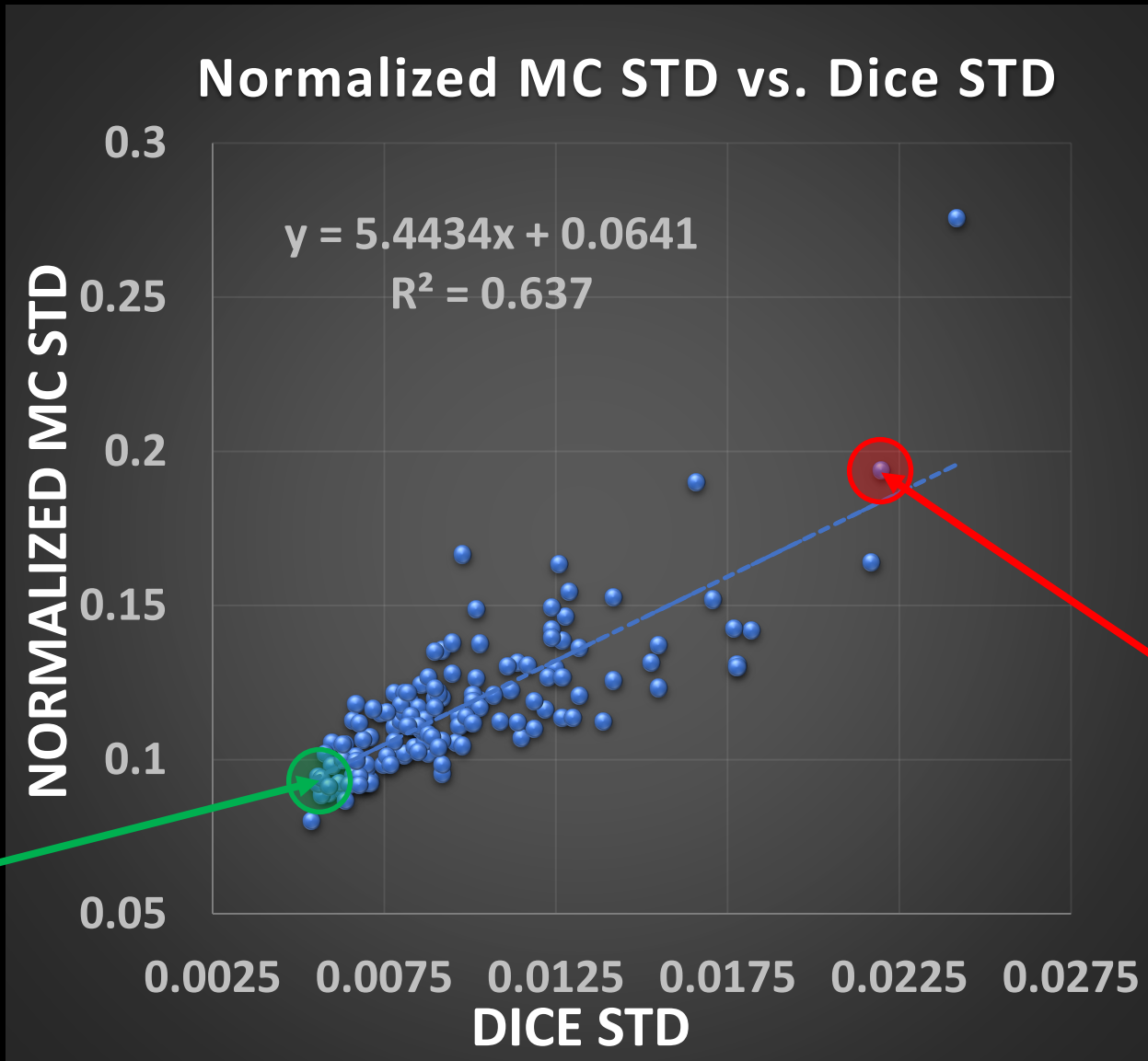
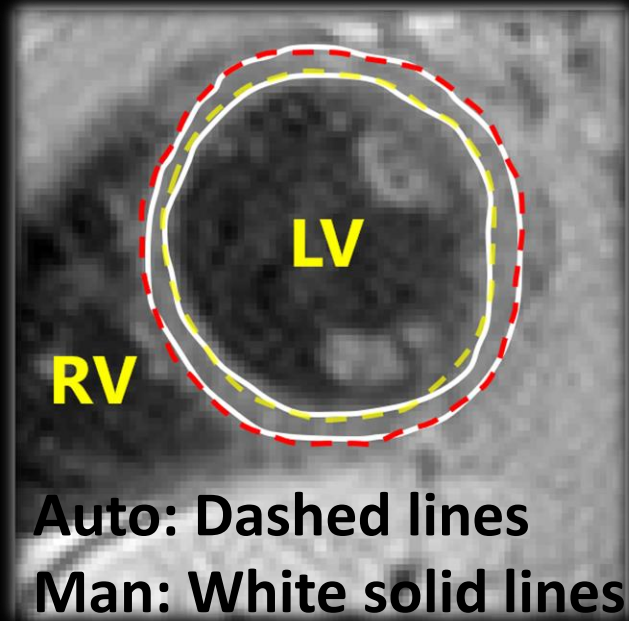


Given man. segmentation

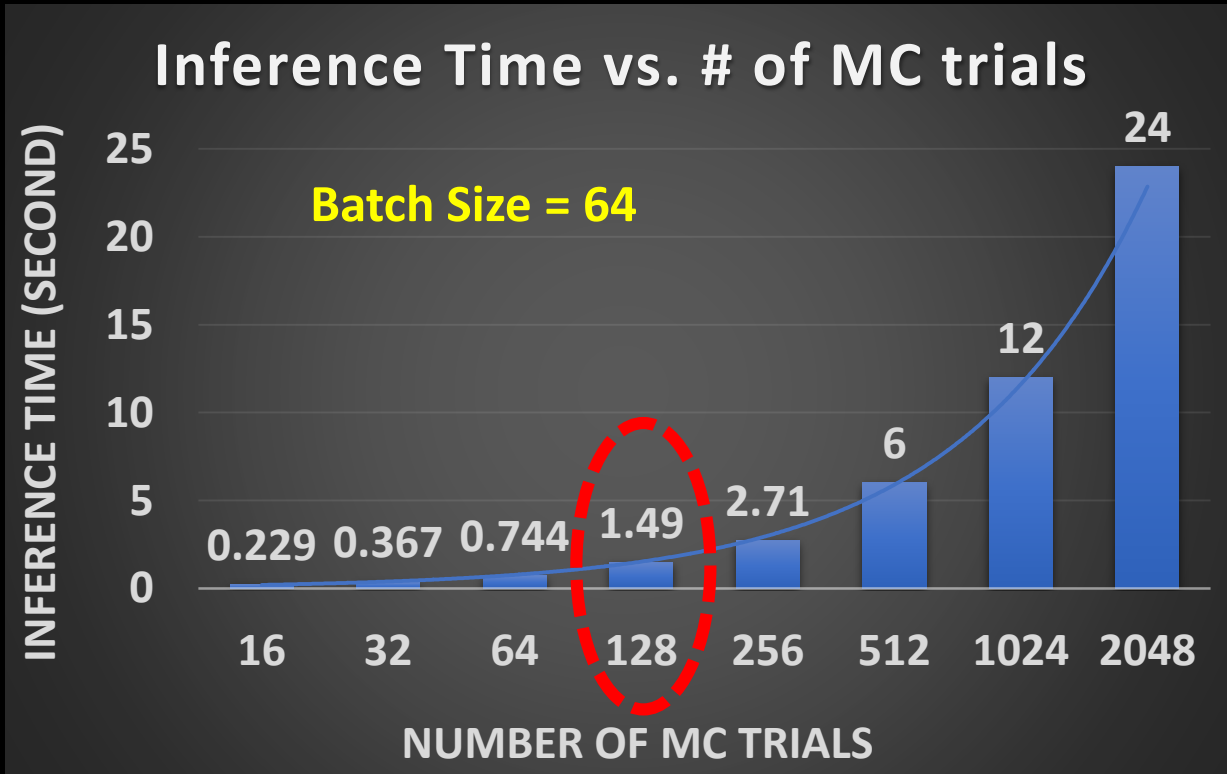


Results(2): Uncertainty

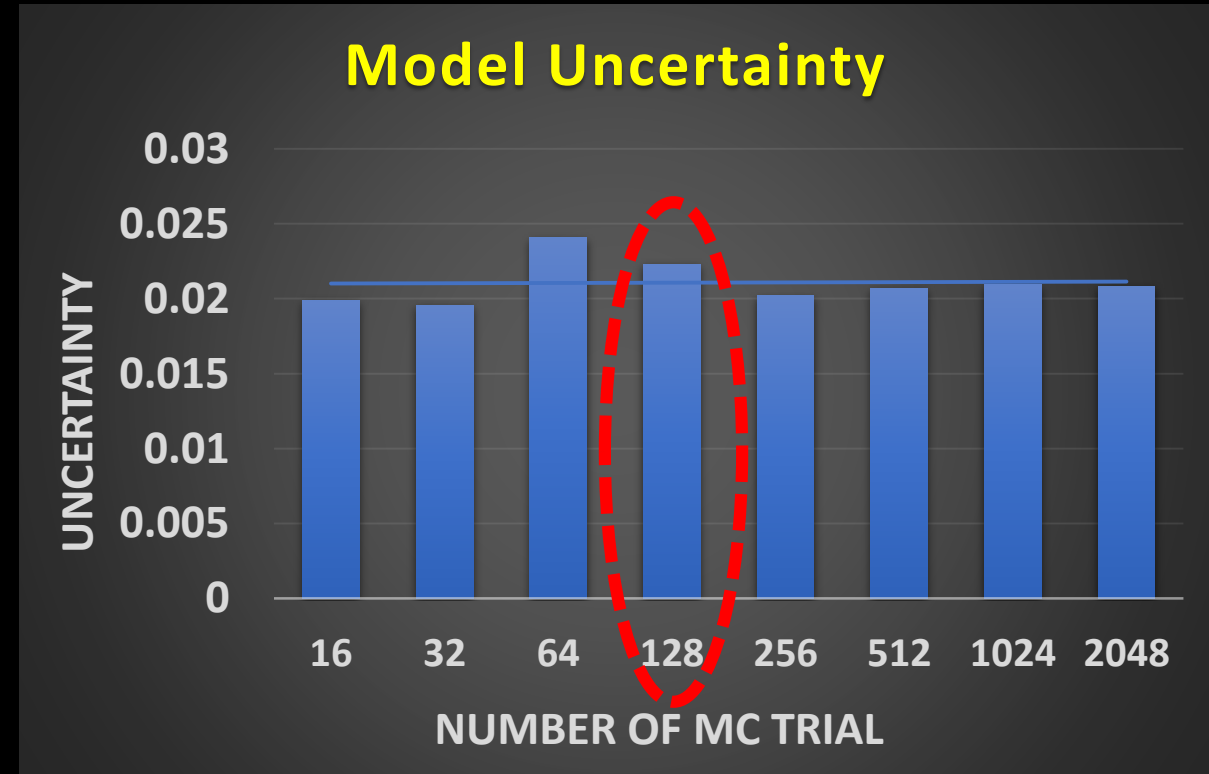
1115 MC trials



Results(2): Uncertainty – Time penalty per image



~1.5s/image with 128 MC trials



Results(3): Adaptability – Partial volume effects

FP = 0
FN ~300 pixels/im

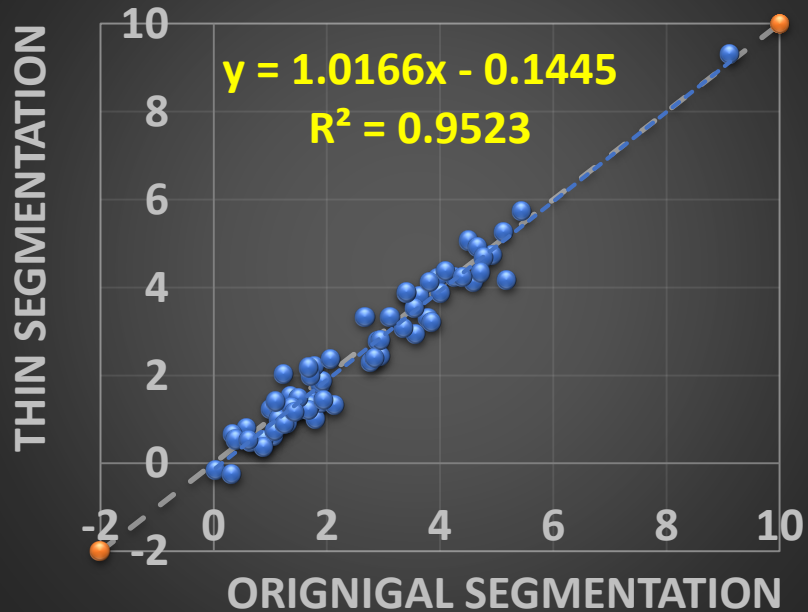
Dice = 0.80 ± 0.04



FP ~400 pixels/im
FN = 0

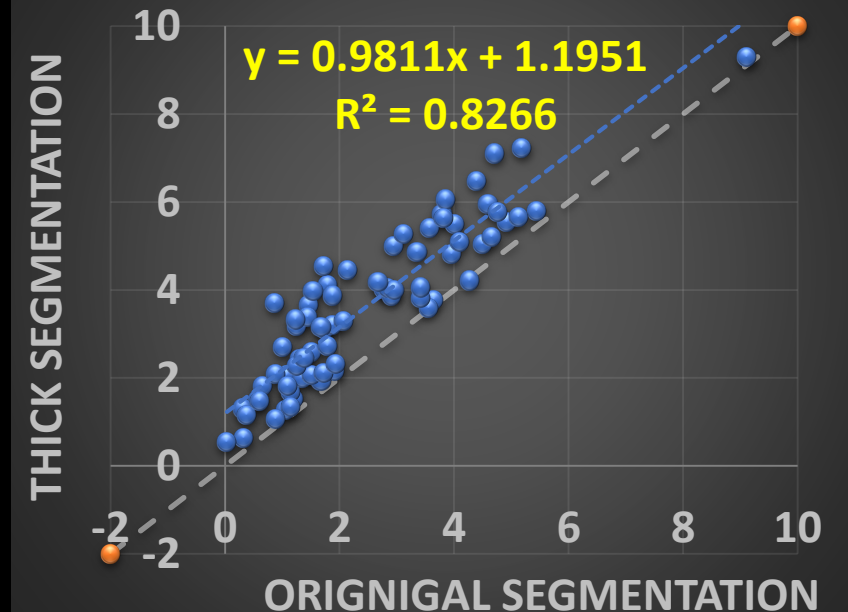
Dice = 0.81 ± 0.02

Regional MBF: Thin vs. Orig.



Significant
overestimation
due to partial
volume effects

Regional MBF: Thick vs. Orig.



Results(3): Adaptability – desired FP and FN trade-off

Diamonds: Thick masks

FP ~400pixels/image

FN = 0

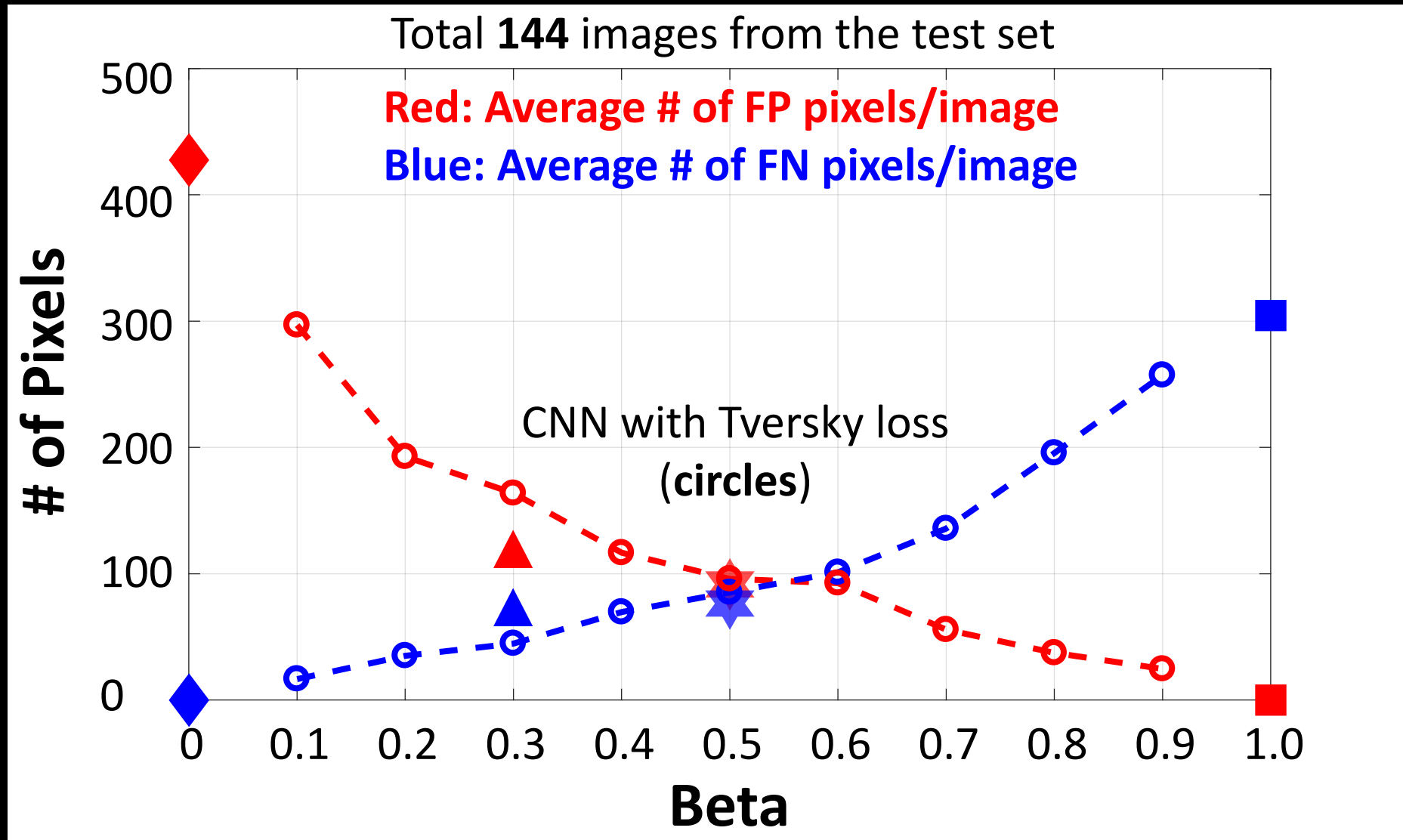
Triangles: CNN with Binary Cross-Entropy loss

Stars: CNN with soft-Dice loss

Squares: Thin masks

FP = 0

FN ~300pixels/image

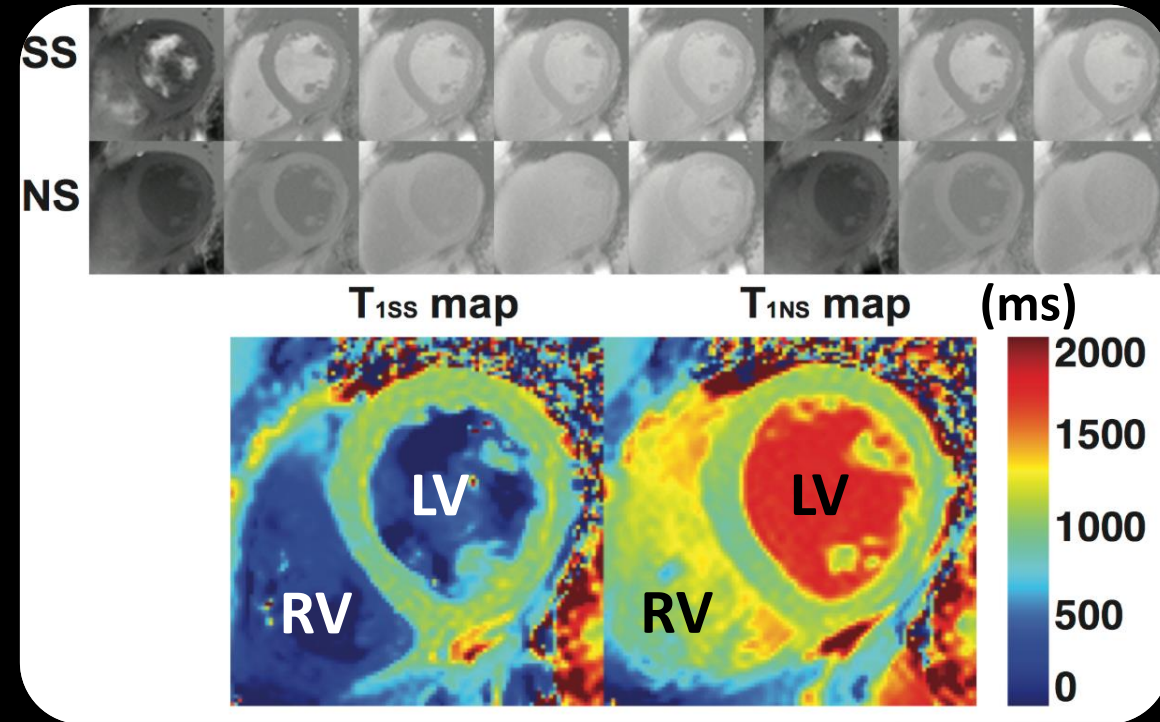
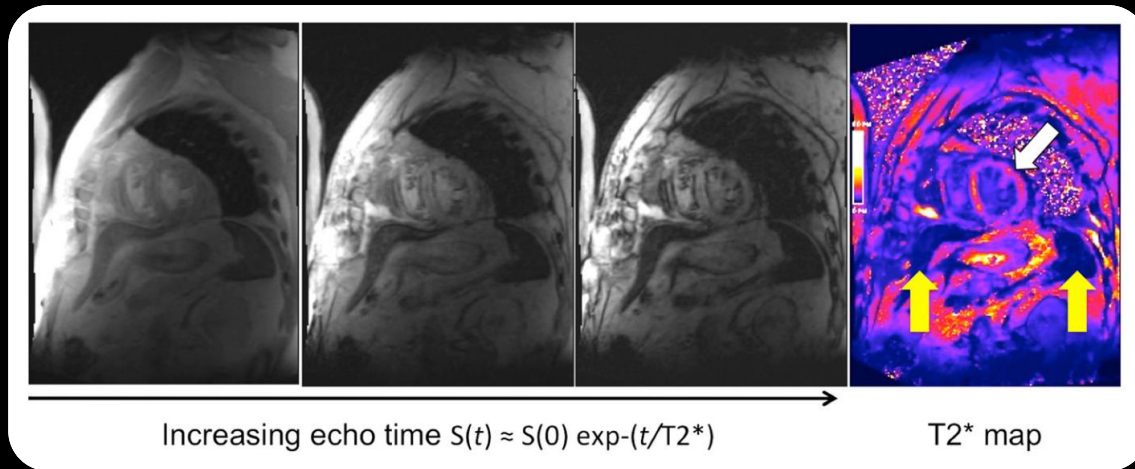


Discussion and Conclusions

- Feasibility to train the CNN model on data with **low and varying SNR and CNR**
- Ability to estimate **model uncertainty** for **quality control and active learning**
- Ability to **adapt** the network to the **desired False Positive and False Negative tradeoff**

→ Applicable to other quantitative CMR:

- **First-pass, T1, T2, T2*, T1rho, DTI, MTR, MRE, etc.**



1. Do, Hung et al. "Myocardial ASL Perfusion Imaging using MOLLI." Proc. ISMRM 24th Scientific Sessions, Singapore, May 2016, p3142.

2. Alam, Shirjel et al. "Vascular and plaque imaging with USPIO." *Journal of Cardiovascular Magnetic Resonance* 17.1 (2015): 83.

Acknowledgements

- Funding:
 - Whittier Foundation
 - NIH/NHLBI, #1R01HL130494-01A1

Canon

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Thank you for your attention!

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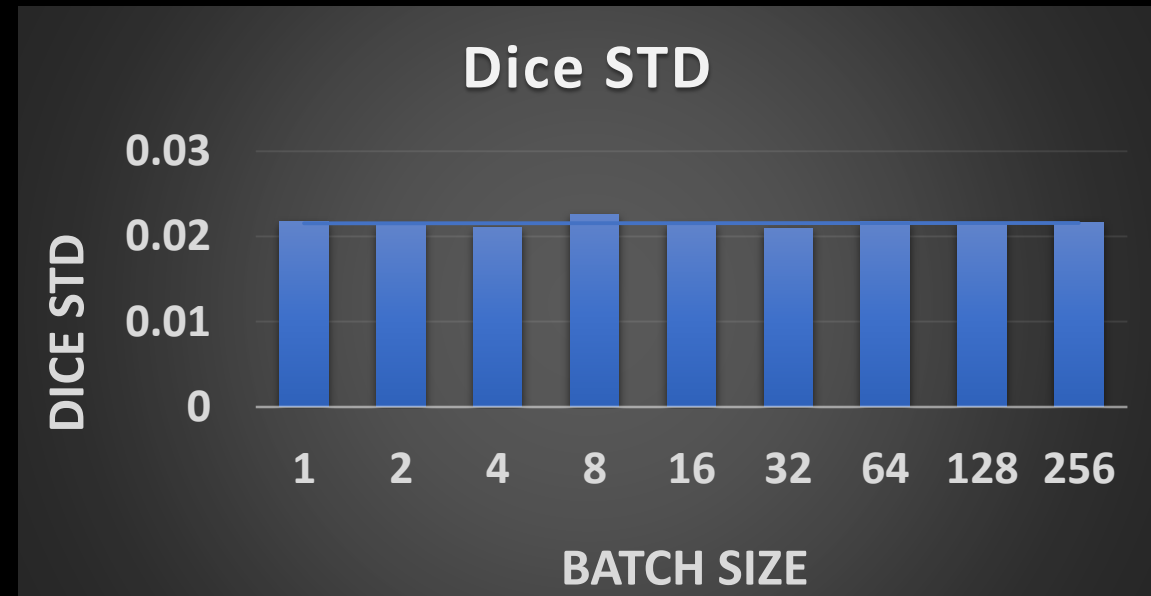
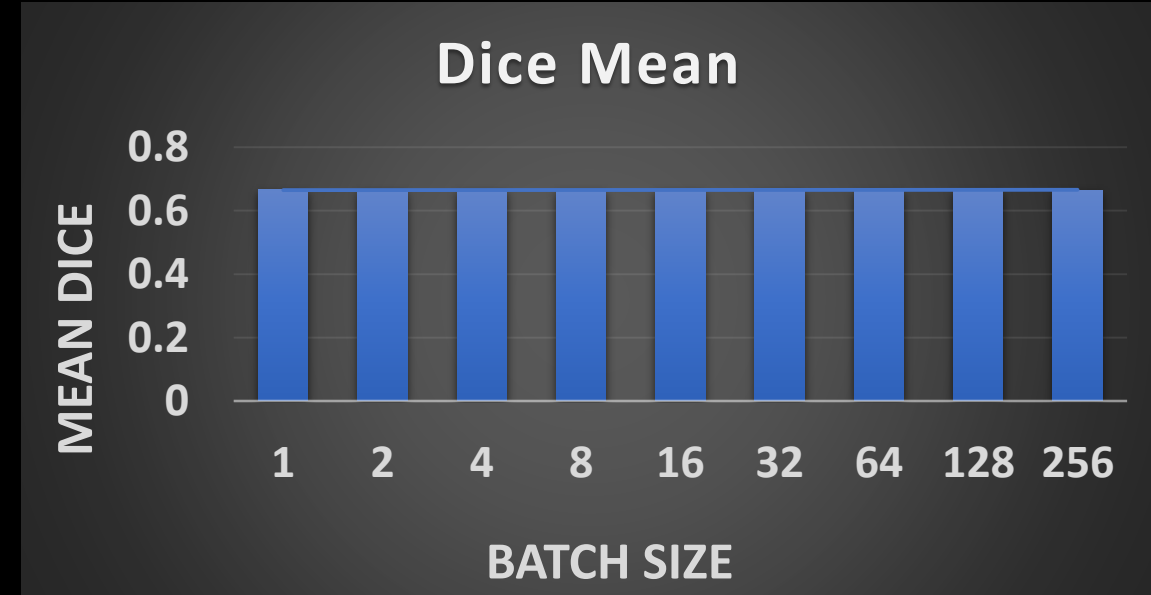
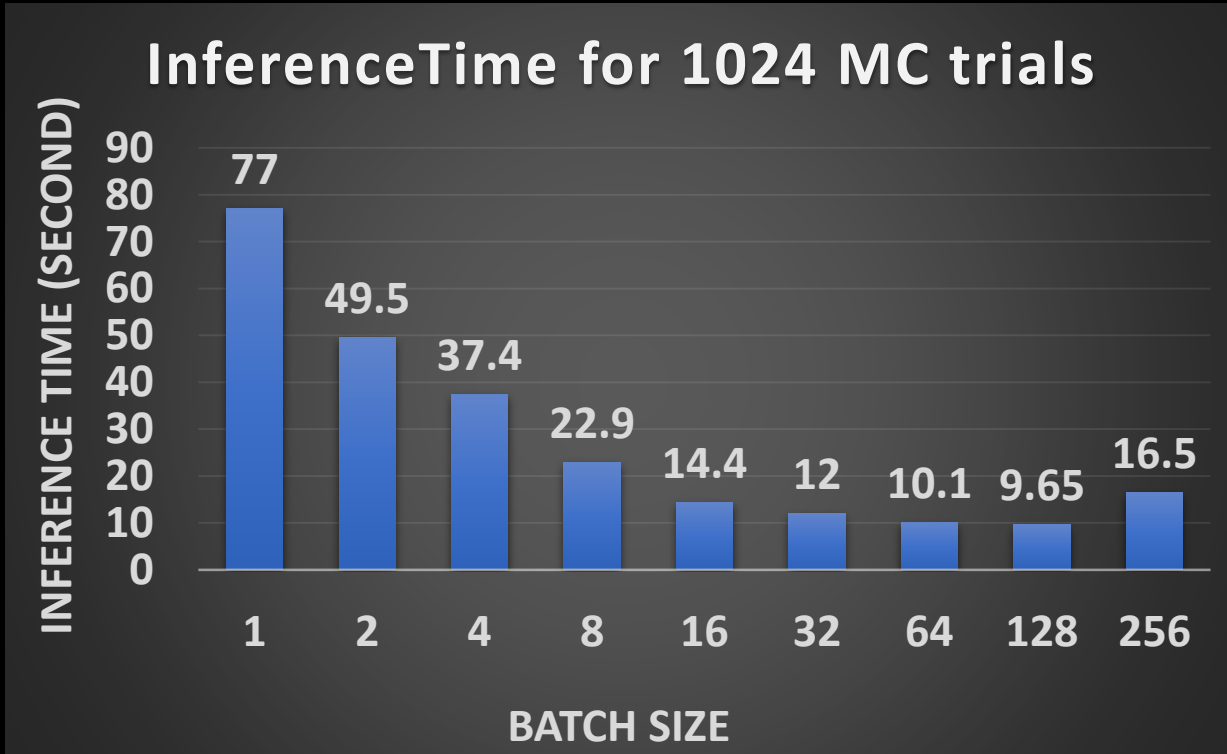
For over 100 years, the Canon Medical Systems `Made for Life' philosophy prevails as our ongoing commitment to humanity. Generations of inherited passion creates a legacy of medical innovation and service that continues to evolve as we do. By engaging the brilliant minds of many, we continue to set the benchmark, because we believe quality of life should be a given, not the exception.

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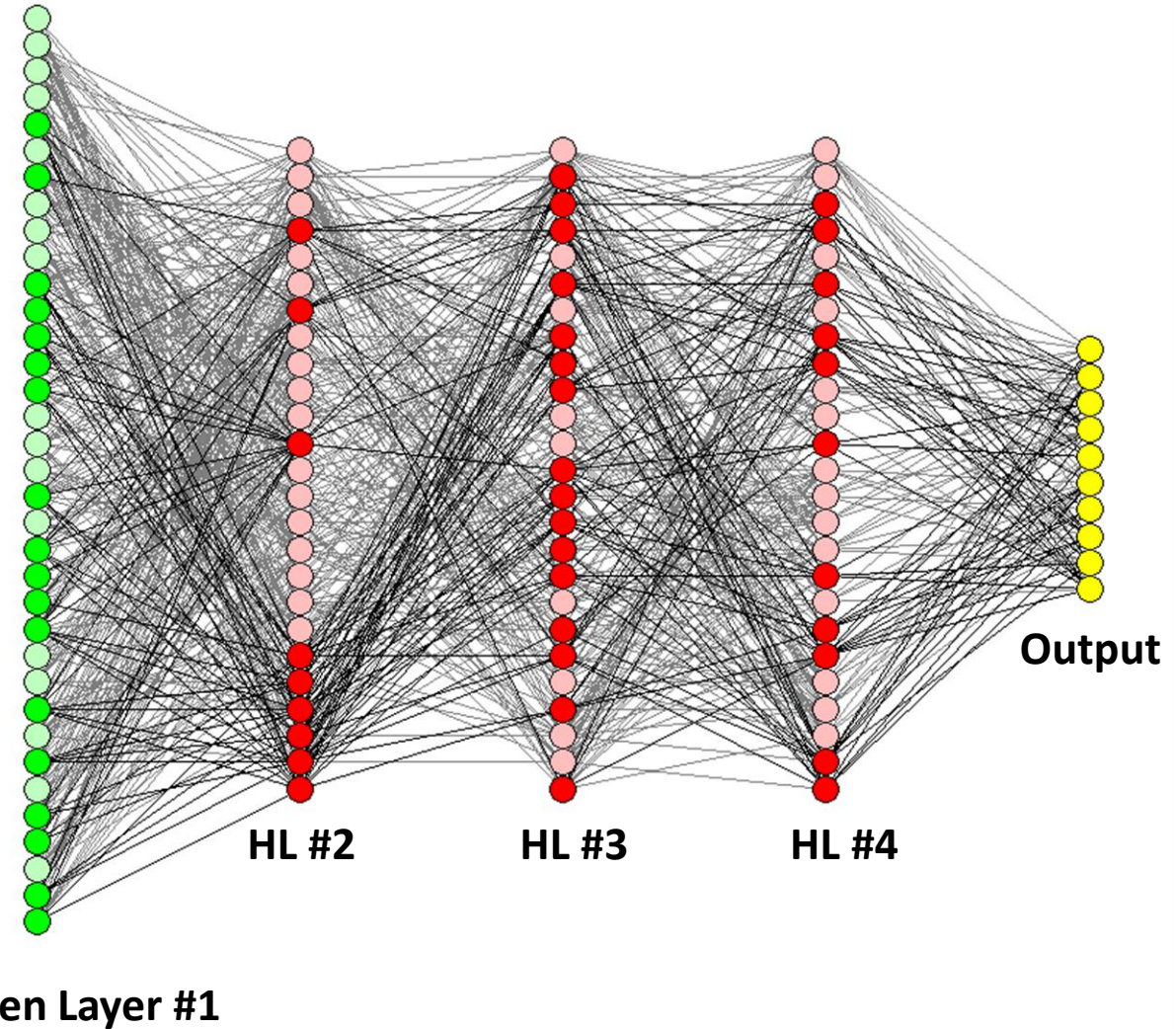
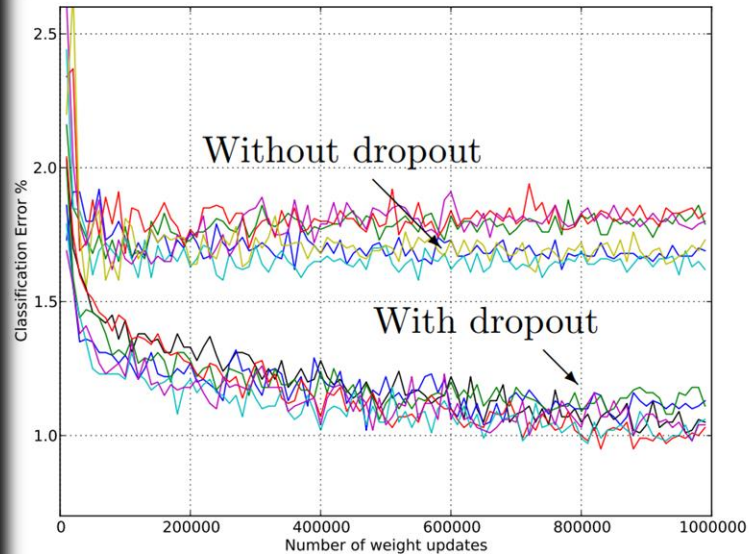
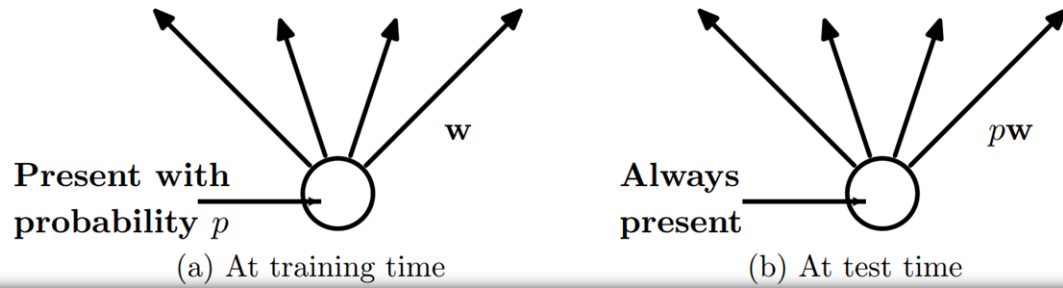
Backup slides

Results(2): Uncertainty – Batch Size



Methods(3): dropout¹

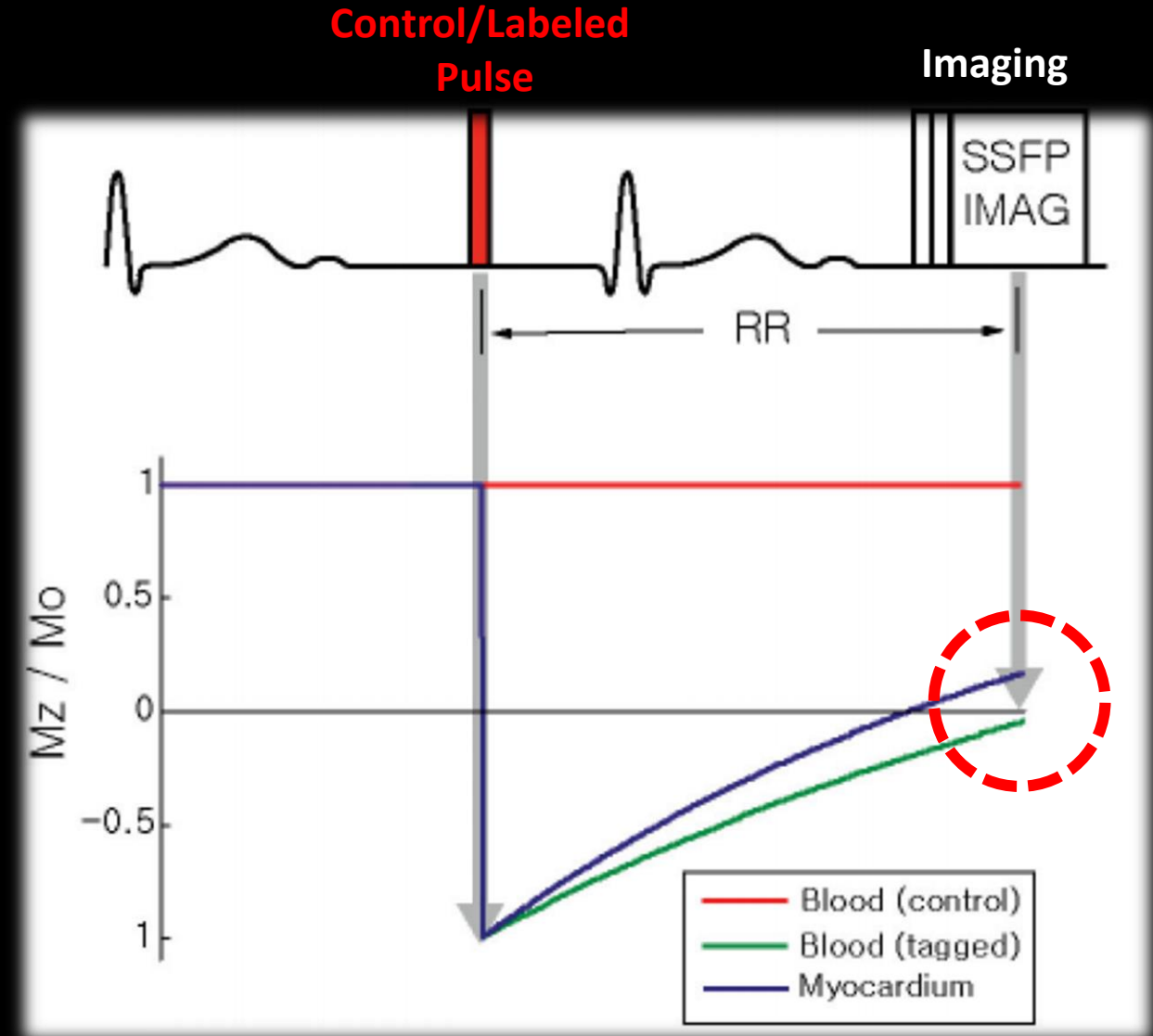
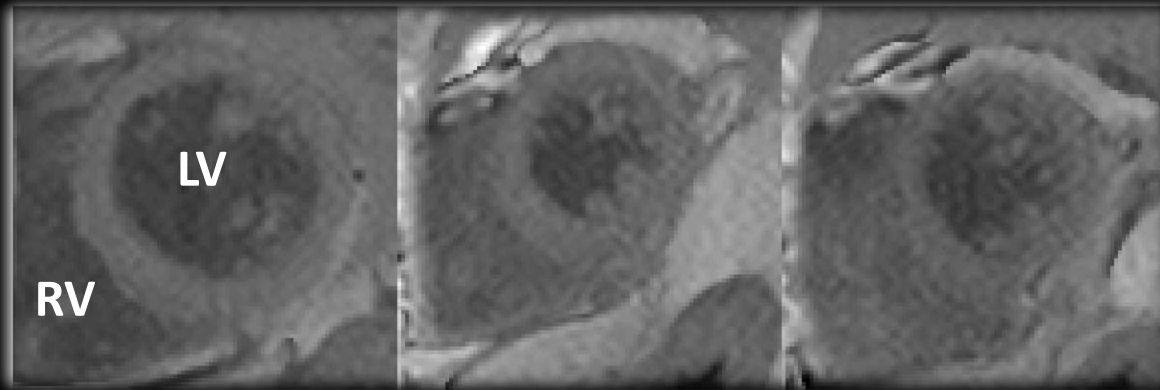
DROPOUT



1. Srivastava et al., "Dropout: A simple way to prevent NN from overfitting." JMLR 2014.
2. Animation is adapted from <https://www.techemergence.com/what-is-machine-learning/>

Intro(3): Data characteristics of ASL

- Low SNR and contrast



Methods(3): Uncertainty measure using MC dropout¹

Dropout as a Bayesian Approximation: Representing Model Uncertainty in Deep Learning

Yarin Gal
Zoubin Ghahramani
University of Cambridge

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ZG201@CAM.AC.UK

- Any NN, with dropout applied before every weight layer, is **mathematically equivalent to an approximation of the Bayesian model.**
- Model uncertainty can be estimated given the **posterior distribution of the trained weights**

Methods(3): Uncertainty measure using MC dropout¹

coursera

Neural Networks for Machine Learning



Lecture 10e

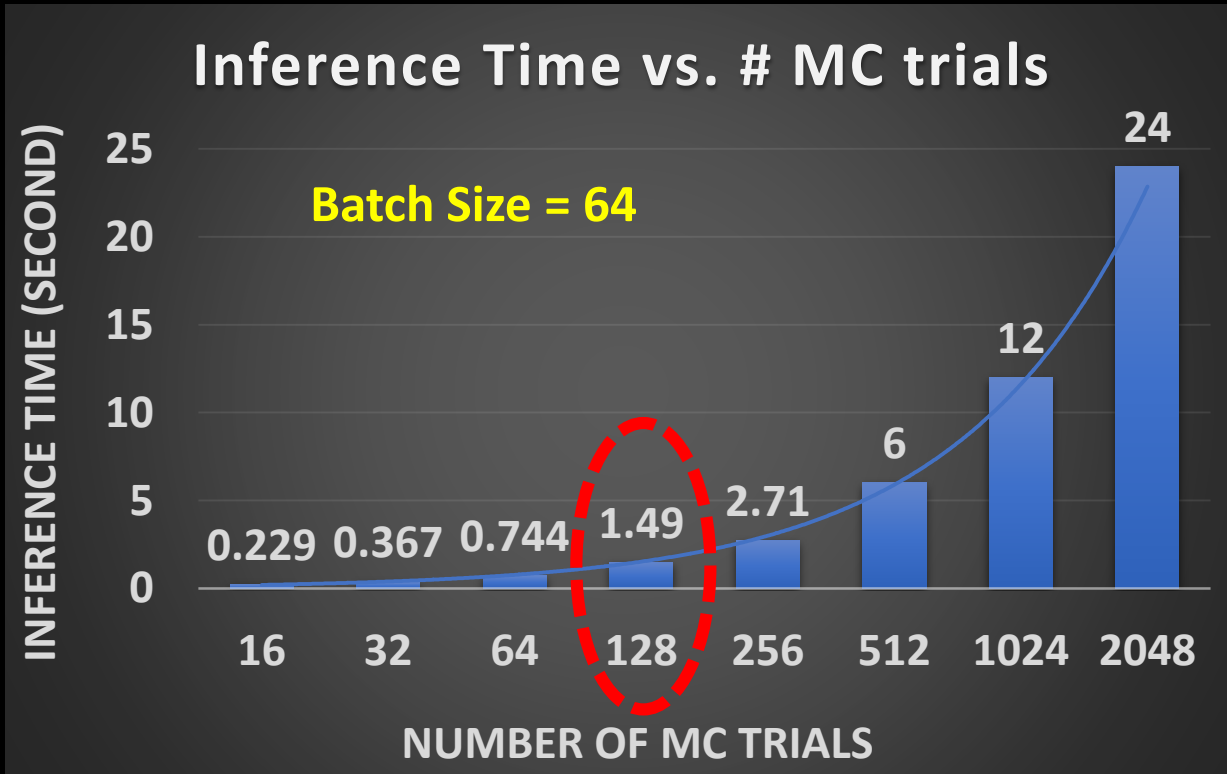
Dropout: an efficient way to combine neural nets

- "Use *dropout of 0.5* in every hidden layer"
- "At test time, *run the stochastic model several times on the same input*"

1. Srivastava et al., "Dropout: A simple way to prevent NN from overfitting." JMLR 2014.

2. Hinton, Geoffrey, "Lecture 10.5 – Dropout: An efficient way to combine neural nets." COURSERA: Neural Networks for Machine Learning 2012: 33-41.

Results(2): Uncertainty – Time penalty



~1.5s/image with 128 MC trials

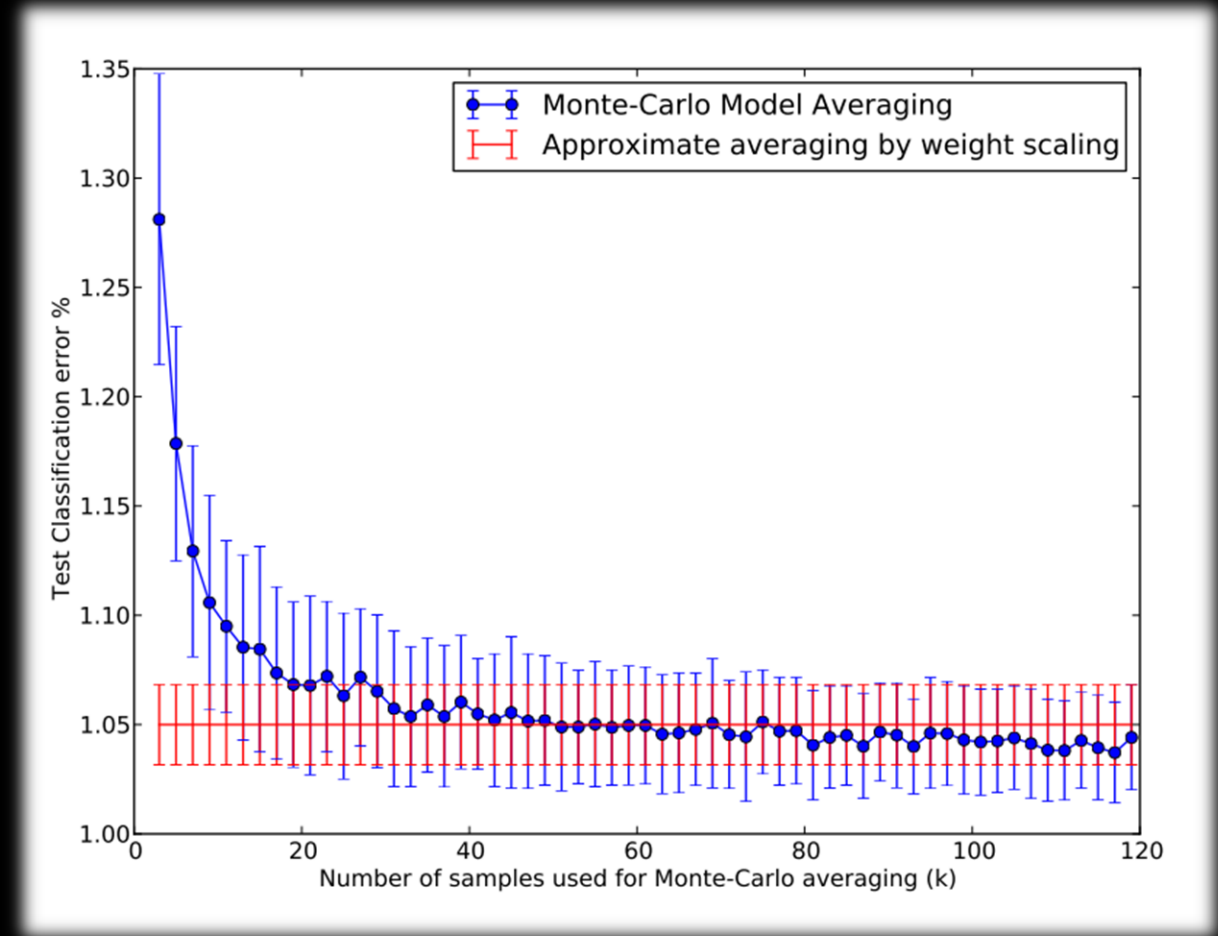


Figure 2: worst and best

